

Optimization of radiation therapy treatment plans

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Outline

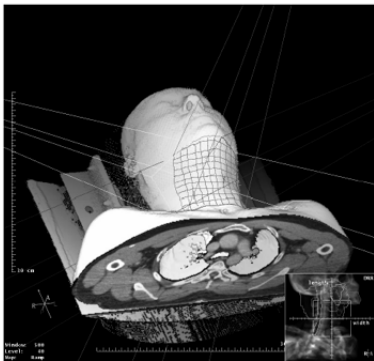
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Radiation therapy and cancer

- Each year, more than 10 million people worldwide are newly diagnosed with cancer
 - about 50-65% of these will be treated by some form of radiotherapy
 - about half of these will benefit from *external beam conformal radiotherapy*
- Despite sophisticated radiation therapy delivery technology
 - many patients still die from their disease
 - others suffer significant side-effects of their treatment
- Better treatment planning and treatment paradigms have the potential to significantly improve patient outcomes

Radiotherapy treatment

- During radiotherapy, beams of radiation pass through a patient, killing not only cancerous but also normal, healthy cells

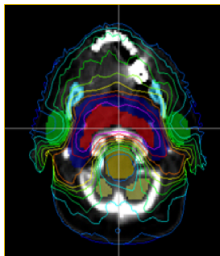


Radiotherapy side effects

- Head-and-neck cancer
 - Delivering too much dose across the spinal cord has the same effect as cutting it
 - Preserving salivary gland function is very important to the quality of life of the patient as well
 - this function allows eating, speaking, maintaining oral hygiene
- Prostate cancer
 - Bowel complications (bleeding, inflammations) should be avoided
- Lung cancer
 - Overdosing the lung may cause a fatal buildup of fluid

Radiotherapy goals

- The goal is to design a treatment plan that
 - delivers a prescribed dose to *targets*
 - while sparing, to the greatest extent possible, *critical structures*
- Radiation therapy therefore seeks to conform the geometric shape of the delivered dose distribution to the targets



Radiotherapy delivery technique

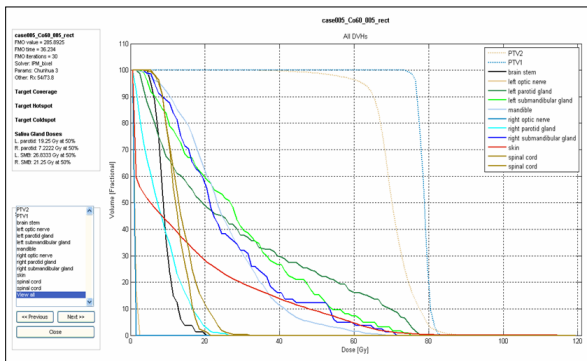
- The currently most widely used delivery technique is called *Intensity Modulated Radiation Therapy (IMRT)*
 - This technique has been used in clinics since 1994
- We will discuss how to build optimization models that can help in the design of a high-quality treatment plan for individual patients
 - Quantifying treatment plan (dose distribution) quality
 - Representation of technological abilities and constraints
 - Radiation vs. dose

Evaluation of dose distribution (1D)

- The physician specifies a collection of measures that summarize the dose distribution *in a given structure* by a single value
- For a target, we may consider
 - minimum dose
 - dose homogeneity (e.g., ratio of maximum to minimum dose)
 - probability of tumor control
- For a critical structure, we may consider
 - (generalized) mean dose
 - maximum dose
 - probability of normal tissue complication

Evaluation of dose distribution (2D)

- The *dose-volume histogram (DVH)* specifies, for each dose value, the fraction of a structure that receives at least that amount of dose



Formal criteria

- The dose distribution is evaluated over a discretization of the irradiated area into a finite number of cubes (*voxels*)
- In particular, we consider a collection of treatment plan evaluation criteria:

$$G_1(z), \dots, G_L(z)$$

expressed as a function of the dose distribution, i.e., the vector of voxel doses z

- smaller values are preferred to larger values

Optimization model: objective

- Multi-criteria optimization

$$\text{minimize } \{G_1(z), \dots, G_L(z)\}$$

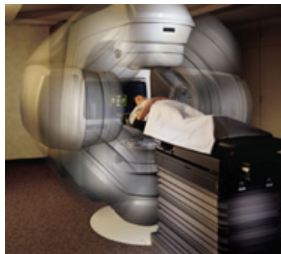
- Single-objective optimization

$$\text{minimize } \sum_{\ell=1}^L w_{\ell} G_{\ell}(z)$$

- We usually avoid imposing *hard constraints* on z

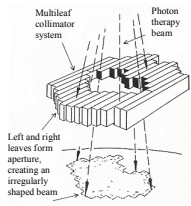
IMRT delivery equipment

- Patients are generally treated on a *linear accelerator*
 - from *multiple directions*



IMRT delivery equipment (2)

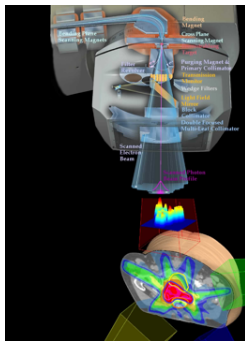
- The intensity (fluence) of the beams can be *modulated*
 - The accelerator is equipped with a *multi-leaf collimator (MLC) system*



- This system can generate *apertures* that shape a beam by blocking part of the radiation

Intensity profile or fluence map

- The superposition of the set of apertures and their intensities
 - corresponds to an *intensity profile* for each beam direction
 - generates a *dose distribution* in the patient



Optimization problem: variables

- Each beam is decomposed into a collection of *beamlets* (*bixels*)
- Beamlet-based models:
 - optimize intensity profile: x_i ($i \in N$)
 - then decompose the profile for each beam into apertures and intensities
- Aperture-based models:
 - optimize aperture intensities: y_k ($k \in K$)

Optimization problem: constraints

- We can predetermine the dose distribution generated by each individual beamlet (or aperture) at unit intensity
- Beamlet-based models:

$$z_j = \sum_{i \in N} D_{ij} x_i \quad j \in V$$

$$x_i \geq 0 \quad i \in N$$

- Aperture-based models:

$$z_j = \sum_{k \in K} D_{kj} y_k \quad j \in V$$

$$y_k \geq 0 \quad k \in K$$

Beamlet vs. aperture-based models

- The mathematical form of beamlet-based and aperture-based models is identical
- Beamlet-based models:
 - Pro: Fewer decision variables
 - Cons: Need for rounding and decomposition; approximate dose distribution
- Aperture-based models:
 - Pro: More accurate computation of dose distribution
 - Con: Large number of variables

Beamlet vs. aperture-based models

- The models are equivalent if

$$D_{kj} = \sum_{i \in A_k} D_{ij}$$

where A_k is the set of beamlets exposed in aperture k

- However, this disregards (for example):
 - Transmission
 - Tongue-and-groove effect
- Moreover, using a beamlet-based approach it is not possible to make a formal trade-off between treatment time and quality

Solving aperture-based models

- We can deal with the large number of decision variables (deliverable apertures) by using a column generation approach
 - provided that the treatment plan evaluation criteria are convex
- In this approach we iteratively
 - Solve a restricted problem with a relatively small number of apertures
 - Solve a pricing problem that
 - either determines that the current solution is optimal
 - or provides an aperture that may improve the solution

Pricing problem

- The pricing problem takes the form

$$\max_{k \in K} \sum_{j \in V} D_{kj} \hat{\pi}_j = \max_{k \in K} \sum_{i \in A_k} \left(\sum_{j \in V} D_{ij} \hat{\pi}_j \right)$$

where

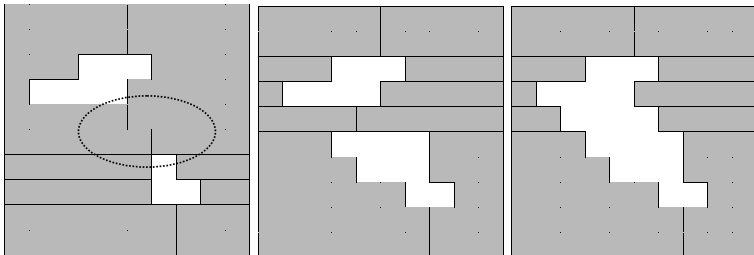
$$\hat{\pi}_j = \sum_{\ell=1}^L w_{\ell} \frac{\partial G_{\ell}(\hat{z})}{\partial z_j}$$

and \hat{z} is the solution to the current restricted problem

- The pricing problem therefore identifies the aperture for which the rate of improvement in the objective function when increasing the aperture intensity is largest

MLC delivery constraints

- Consecutiveness
- Non-interdigitation
- Connectedness
- Jaws-only



Pricing problem (2)

- We can formulate a DP algorithm that solves the pricing problem in polynomial time
 - Associate a node with all possible leaf settings for all rows of the MLC
 - Connect nodes corresponding to adjacent leaves, maintaining feasibility
- In some cases (consecutiveness; jaws-only) a more efficient algorithm can also be found

Pricing problem (3)

- Examples of extensions:
- *Transmission:*

$$D_{kj} = \sum_{i \in A_k} D_{ij} + \epsilon \sum_{i \in \bar{A}_k} D_{ij}$$

- *Treatment efficiency:*
Include a term in the objective that penalizes total beam-on-time:

$$\sum_{k \in K} y_k$$

Current treatment paradigm

- *Day 1*
 - Image patient anatomy (CT, MRI, PET scan)
- *Days 2–5*
 - Contour targets and critical structures
 - Generate problem data
 - Determine “optimal” treatment plan
- *Day 6–40*
 - Treat patient in 35 daily *fractions*

Interfraction motion

- Patient needs to be set up at the linear accelerator for each fraction
 - This cannot be done with complete precision
 - Setup errors mean that the actual delivered dose distribution on a given treatment day differs from the planned/optimized one
- Even if the patient could be repositioned *exactly* on each treatment day, the delivered dose distribution would still not be the same for each fraction
 - Organ motion
 - Tumor shrinkage/growth
 - Patient weight loss

Interfraction motion (2)

- Periodic reoptimization:
 - Collect data by more frequently imaging patient
 - Process data after treatment
 - Re-plan based on delivered dose

Unresolved issue

- How should dose be added between fractions?
 - Acute effects
 - Late effects
- New biological models are required to assess the effect of delivering nonstationary dose distributions

Intrafraction motion

- Each treatment fraction takes about 10 minutes
- During a single fraction the patient moves because of
 - breathing
 - swallowing
 - bladder filling

Intrafraction motion

- Currently the consequences of intrafraction motion is unknown
- We need so-called 4D image sets (“movies”) of the patient during treatment
- Tasks:
 - Assess effects of intrafraction motion for various disease sites
 - Modify treatment plan (optimization) accordingly where needed

Image-guided radiotherapy

- By more frequently imaging the patient we may learn about motion and correct for it
- *Image-Guided IMRT (IGIMRT)*
- Several manufacturers are already offering radiation equipment that allows for more frequent imaging – but this is currently mainly limited to helping with patient setup

Information

- More and more frequent imaging of patients will lead to a large amount of additional information
- How can we make the best use of this information, i.e., how can we find the *optimal* treatment plan (strategy) for each patient given this information?
- Which type(s) of information provide the largest benefit to the patient?

Conclusions

- The problem of efficiently finding a high-quality *static* treatment plan based on a *single image set* and assuming *stationarity* of the patient is relatively well-solved
- However, we need to better deal with *uncertainties* and *nonstationarities*
- Operations research can help:
 - make optimal use of available technology
 - help assess which potential future technological enhancements are most valuable to the patient